Sensitivity Enhancement in Solid-State ¹³C NMR of Synthetic Polymers and Biopolymers by ¹H NMR Detection with High-Speed Magic Angle Spinning

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Indirect detection of ¹³C and ¹⁵N nuclear magnetic resonance (NMR) spectra through ¹H NMR signals offers large sensitivity advantages in studies of organic and biological molecules in solution and is almost universally employed.¹⁻³ Although sensitivity enhancement by indirect detection was first demonstrated in NMR⁴⁻⁶ and nuclear quadrupole resonance^{7,8} of solids, direct detection has generally been preferred in solid-state NMR.⁹ This is because the broad ¹H NMR lines of organic solids negate sensitivity enhancement under the most common conditions. We have recently shown¹⁰ that substantial sensitivity enhancements can in fact be achieved by indirect detection in one-dimensional (1D) solid-state ¹⁵N NMR spectroscopy of organic compounds and biopolymers under magic angle spinning (MAS) at speeds that greatly reduce the ¹H NMR line widths.¹⁰⁻¹² Here we demonstrate the feasibility of sensitivity enhancement in solidstate ¹³C NMR spectroscopy of general organic solids. We present experimental results both for the noncrystalline synthetic polymer poly(methyl methacrylate) (PMMA) and for the heptapeptide *N*-acetyl-Lys-Leu-Val-Phe-Phe-Ala-Glu-NH₂ (A β_{16-22} , representing residues 16 through 22 of the 40-residue Alzheimer's β -amyloid peptide¹³) in the form of amyloid fibrils. We report enhancements in both 1D and two-dimensional (2D) experiments. Extension to ¹³C NMR, which forms the basis for many structural and dynamical studies in organic and biological systems, and to 2D spectroscopy significantly broadens the impact and generality of indirect detection methods in solid-state NMR.

The sensitivity enhancement factor ξ , defined as the ratio of frequency-domain signal-to-noise ratios for 1H-detected and 13Cdetected measurements, is given by

$$\xi = \left(\frac{f^2 d}{\alpha}\right)^{1/2} \left(\frac{\gamma_{\rm H}}{\gamma_{\rm C}}\right)^{3/2} \left(\frac{W_{\rm C}}{W_{\rm H}}\right)^{1/2} \left(\frac{Q_{\rm H}}{Q_{\rm C}}\right)^{1/2} \frac{A_{\rm H}}{A_{\rm C}}$$

where γ is the magnetogyric ratio, W is the effective line width, Q is the quality factor of the sample coil, and A subsumes properties such as coil geometry, filling factor, receiver noise

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Figure 1. 2D ¹³C/¹H heteronuclear correlation spectra of PMMA powder (9 mg, unlabeled) obtained with ¹³C detection (a, c, e, g) and with ¹H detection (b, d, f, h). 1D slices are shown at ¹H shifts of 0.9 (c, d), 3.7 (e, f), and -3.5 ppm (g, h). See Figure 2 for ¹³C assignments. The ¹³Cdetected spectrum is obtained with the rf pulse sequence $90^{H}_{\phi} - t_1^{H} - CP_x$ $t_2^{\rm C}$. The ¹H-detected spectrum is obtained with the sequence $90^{\rm H}_{\nu}$ – CP_x– $t_1^{\rm C}-90^{\rm C}_{\phi}-\tau_{\rm d}-90^{\rm C}_{\rm v}-{\rm CP}_x-t_2^{\rm H}$, where 90 is a $\pi/2$ pulse, CP is a 2 ms cross polarization period, t_1 is the evolution period, τ_d is a 5 ms period for dephasing of transverse ¹³C magnetization and ¹H magnetization suppression (see text), and t₂ is the detection period. Superscripts H and C indicate ¹H and ¹³C. Subscripts x, y, and ϕ indicate rf phases, with $\phi =$ x and y for quadrature detection in t_1 . ¹H rf field amplitudes are 71 kHz for CP and 8 kHz for decoupling during t_1^{C} or t_2^{C} . The ¹³C rf field amplitude is swept from 50 to 30 kHz with a tangent shape during CP. No ¹H-¹H decoupling is applied during CP, so that each ¹H signal correlates with multiple ¹³C signals. A total of 528 scans are acquired for each of spectra a and b. Lorentzian broadening of 390 Hz in the 13C dimension and 770 Hz in the ¹H dimension is applied. Maximum t_1^{C} and $t_2^{\rm H}$ (or $t_2^{\rm C}$ and $t_1^{\rm H}$) values are 1.28 and 0.65 ms, respectively.

figure, and lead loss.^{10,14} The symbols H and C refer to the ¹H and ${}^{13}C$ nuclei, f is the efficiency of polarization transfer between 13 C and 1 H spins, and d is the receiver duty factor for indirect detection (see below). When the ¹H-detected and ¹³C-detected measurements have the same dimensionality, $\alpha = 1$. When the ¹³C-detected measurement is 1D but the ¹H-detected measurement is 2D, $\alpha \approx 2\pi$ because of signal decay and the need for quadrature detection in the t_1 dimension.^{10,14} Typically, $A_{\rm H}/A_{\rm C} \approx 1$, $Q_{\rm H}/Q_{\rm C}$ \approx 2, and $\gamma_{\rm H}/\gamma_{\rm C}$ = 3.98, but in the absence of high-speed MAS or other line-narrowing techniques, $W_{\rm C}/W_{\rm H} < 0.01$ and consequently $\xi < 1$. Under MAS at sample rotation frequencies $v_{\rm R} \ge$ 30 kHz and ¹H NMR line widths are reduced approximately from 50 to 1 kHz. Then, for $W_{\rm C} = 300$ Hz and f = 0.5, we find $\xi \approx$ $3.1(d/\alpha)^{1/2}$ and sensitivity enhancement appears possible.

Figure 1 compares 2D ¹³C/¹H heteronuclear correlation (HET-COR) spectra of PMMA powder obtained with conventional ¹³C detection and with ¹H detection. These spectra are acquired at 17.6 T (749.5 and 188.5 MHz 1H and 13C NMR frequencies) and

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Figure 2. 1D ¹³C NMR spectra of PMMA powder (4.5 mg, unlabeled) obtained with ¹³C detection (a) and with ¹H detection (b). Total of 344 scans for each spectrum. Spectrum a is obtained in a 1D manner with CP and decoupling conditions as in Figure 1. Spectrum b is a single slice of a 2D spectrum obtained with the conditions in Figure 1b, but with a pulse spin locking (PSL) train applied in the t_2^{H} period and with $\tau_d = 4$ ms. The PSL train consists of one 6 $\mu s \pi/2$ pulse with phase *x* per sample rotation period. Complex ¹H signal points are sampled every 0.5 μs during 14 μs windows between PSL pulses.

 $v_{\rm R} = 31000 \pm 5$ Hz, with identical total acquisition times. Experimental ξ values are up to 3.3 for protonated carbon and 1.6 for the nonprotonated carbon signals. ¹³C-detected HETCOR measurements^{15,16} are widely used as a means of resolving and assigning ¹³C and ¹H chemical shifts in studies of synthetic polymers¹⁷ and biological compounds.^{12,18} The results in Figure 1 suggest that reductions in acquisition times by a factor of 10 may be possible in many cases through ¹H detection and high-speed MAS.

Figure 2 compares 1D ¹³C NMR spectra of PMMA obtained at $v_{\rm R} = 31250 \pm 5$ Hz and 17.6 T with conventional ¹³C detection and with ¹H detection. In this case, because the ¹³C-detected measurement is 1D but the ¹H-detected measurement is necessarily 2D, ξ is reduced by the factor $\alpha^{1/2}$. To compensate for this reduction, ¹H signals are detected with pulsed spin-locking (PSL),¹⁹ i.e., ¹H signals are sampled in windows between rotor synchronized radio frequency (rf) pulses that reduce the effective ¹H line width to roughly 50 Hz. Because of the finite pulse lengths and receiver dead time, the sampling windows comprise a fraction d = 0.438 of the total acquisition time. ¹H chemical shift information is lost under PSL, but this information is also absent in the 1D ¹³C-detected measurement. For quaternary and protonated ¹³C sites, $\xi \approx 2.5$ in Figure 2. For the carbonyl site, $\xi \approx$ 1.5.

The PMMA samples in Figures 1 and 2 are not ¹³C-labeled. A potential pitfall in ¹H-detected ¹³C NMR measurements, especially at natural abundance, is the large " t_1 noise"¹⁴ contributed by ¹H nuclei that do not participate in polarization transfer to ¹³C nuclei. To obtain the sensitivity enhancements described above, we apply two 400 μ s rf pulses at the ¹H NMR frequency, with phases *x* and *y* and with amplitudes set to $v_R/2$ for rotary resonance recoupling,²⁰ during the ¹³C dephasing period τ_d (see Figure 1 caption). These pulses destroy ¹H magnetization that would otherwise generate t_1 noise.

Figure 3 compares ¹³C-detected and ¹H-detected ¹³C/¹H HET-COR spectra of A β_{16-22} fibrils obtained at $v_{\rm R} = 31250 \pm 5$ Hz and 17.6 T. Ten percent of A β_{16-22} molecules are ¹³C-labeled at

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Figure 3. 2D ¹³C/¹H heteronuclear correlation spectra of amyloid fibrils formed by the heptapeptide $A\beta_{16-22}$ (2 mg, lyophilized powder; peptides uniformly ¹³C-labeled in the central five amino acid residues are diluted to 10% in unlabeled peptides) obtained with ¹³C detection (a, c, e, g) and with ¹H detection (b, d, f, h). 1D slices are shown at ¹H shifts of 0.7 (c, d), 6.9 (e, f), and 13.0 ppm (g, h, vertical scale increased to show noise level). Experimental conditions are the same as in Figure 1 but τ_d = 6.5 ms, maximum t_1^C and t_2^H (or t_2^C and t_1^H) values are 1.50 and 0.75 ms, and 9726 total scans per spectrum. Lorentzian broadening of 335 Hz in the ¹³C dimension and Gaussian broadening of 675 Hz in the ¹H dimension are applied.

all carbon sites in the central five hydrophobic residues.¹³ ξ values are up to 2.4 for protonated and 1.8 for nonprotonated ¹³C signals. Although the sharper ¹³C lines in A β_{16-22} fibrils lead to smaller ξ values than in Figure 1, these results still indicate a reduction of data acquisition time by a factor of 5.

The spectrum in Figure 3b provides new constraints on the structure of $A\beta_{16-22}$ amyloid fibrils. ¹³C chemical shift assignments, initially determined from ¹³C/¹³C 2D exchange spectra,¹³ are confirmed by the present data. Additionally, ¹H chemical shifts determined from Figure 3b (5.1, 4.7, 5.1 ppm ¹H_{α} shifts for Leu17, Val18, and Ala21, respectively, ±0.3 ppm precision; 1.2 and 0.8 ppm ¹H_{β} shifts for Leu17 and Ala21) support a β -strand backbone conformation for the labeled residues.²¹ ¹H_{α} (5.8 ppm) and ¹H_{β} (1.6 and 3.2 ppm) shifts for Phe residues and the ¹H_{β} (1.2 ppm) shift for Val18 are anomalous,²¹ possibly indicating intermolecular contacts between Phe and Val residues in a laminated β -sheet structure.¹³

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Supporting Information Available: Table of chemical shifts from Figure 3 and expansion of Figure 3b with assignments (PDF). This material is available free of charge via the Internet at http://pubs.acs.org.

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